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Accuracy and precision of oscillometric blood pressure in standing conscious horses

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Abstract

Background – Arterial blood pressure (BP) is a relevant clinical parameter that can be measured in standing conscious horses to assess tissue perfusion or pain. However, there are no validated oscillometric noninvasive blood pressure (NIBP) devices for use in horses.

Animals – Seven healthy horses from a teaching and research herd.

Hypothesis/Objective – To evaluate the accuracy and precision of systolic arterial pressure (SAP), diastolic arterial pressure (DAP), and mean arterial pressure (MAP) in conscious horses obtained with an oscillometric NIBP device when compared to invasively measured arterial BP.

Methods – An arterial catheter was placed in the facial or transverse facial artery and connected to a pressure transducer. A cuff for NIBP was placed around the tail base. The BP was recorded during normotension, dobutamine-induced hypertension, and subnormal BP induced by acepromazine administration. Agreement analysis with replicate measures was utilized to calculate bias (accuracy) and standard deviation (SD) of bias (precision).

Results – A total of 252 pairs of invasive arterial BP and NIBP measurements were analyzed. Compared to the direct BP measures, the NIBP MAP had an accuracy of $-4$ mm Hg and precision of $10$ mm Hg. SAP had an accuracy of $-8$ mm Hg and a precision of $17$ mm Hg and DAP had an accuracy of $-7$ mm Hg and a precision of $14$ mm Hg.

Conclusions and Clinical Relevance – MAP from the evaluated NIBP monitor is accurate and precise in the adult horse across a range of BP, with higher variability during subnormal BP. MAP but not SAP or DAP can be used for clinical decision making in the conscious horse.

Keywords: arterial blood pressure, acepromazine, dobutamine, equinen, oninvasive blood pressure

Abbreviations

BP blood pressure
DAP diastolic arterial pressure
IBP invasive arterial blood pressure
MAP mean arterial pressure
NIBP noninvasive blood pressure
SAP systolic arterial pressure

SVR systemic vascular resistance

Introduction

Blood pressure (BP) measurement in critically ill, conscious, standing horses is useful for assessment of dynamic cardiovascular changes related to systemic inflammatory response syndrome (SIRS), septicemia, cardiac failure, endotoxia, hypovolemia, and equine metabolic syndrome. The current reference standard for arterial blood pressure in horses is direct measurement of systolic arterial pressure (SAP) and diastolic arterial pressure (DAP). Mean arterial blood pressure (MAP) is calculated from these values as a real-time estimate of average BP. Although measurement of MAP is the most clinically applicable and readily available technique to assess a patient’s cardiovascular status, arterial BP does not equal arterial blood flow. Mean arterial BP can be calculated by the equation:
MAP (mmHg) = Cardiac Output (L/min) × Systemic Vascular Resistance (dyn/s/cm²) × 80.

Therefore, MAP is affected by the relationship between cardiac output and systemic vascular resistance (SVR). If SVR is increased, MAP may be normal or high, but cardiac output, and therefore blood flow, may be compromised.⁹

Direct or invasive arterial blood pressure (IBP) is rarely measured in the standing horse with clinical disease, despite a negative association between preoperative hypotension and survival in horses with colic.¹⁰ Difficulty in placing and maintaining an arterial catheter in the conscious horse prevents routine use of IBP as a monitoring aid. In addition, direct arterial cannulation of the critically ill patient poses a risk for iatrogenic thrombosis and sepsis¹¹ and requires more training, compared to the easy, safe, and noninvasive application of a noninvasive blood pressure (NIBP) cuff. The use of an oscillometric NIBP monitor has been investigated in anesthetized and conscious foals,¹²,¹³ in anesthetized horses,¹⁴–¹⁶ and standing adult horses.¹⁶ Oscillometry is routinely used in human medicine and small animal veterinary practice but is less commonly used in large animal practice.

Oscillometric BP measurement devices provide objective and automated measurement of MAP, and then calculate the values for SAP and DAP. These devices may have a diagnostic advantage over other indirect methods (eg, Korotkoff sound detection, Doppler ultrasonic flow detection).¹,³ MAP is generally considered to best reflect systemic BP, and SAP is generally used for intraoperative clinical decision making.¹,¹⁷

To the authors’ knowledge, there are no studies investigating the accuracy and precision of oscillometric NIBP in conscious standing horses during clinically relevant hypo- or hypertension. This evaluation is a necessity for the practical application of any device and cannot be transferred across species.¹⁸ The objective of this study was to evaluate the accuracy and precision of oscillometric NIBP during periods of normotension, subnormal BP, and hypertension in healthy conscious standing horses, compared to IBP.

Materials and Methods

Seven trotter mares between 4 and 14 years old (mean age of 9.2 years ± standard deviation [SD] of 3.2 years) weighing between 447 and 612 kg (mean weight of 538 ± 56 kg) were included in this study. Horses belonged to the teaching and research herd at the Department of Large Animal Sciences, University of Copenhagen, and were not pregnant or receiving any medications during the data collection period and were judged to be clinically healthy. Horses were excluded from the study if they were obese or if they demonstrated clinical signs of infection or overt pain. Routine physical examination was performed prior to the initiation of the study (on days −7 and −1), twice daily during the study, and again the day after conclusion of experimental procedures. All experimental procedures were approved by the Institutional Ethics Committee and the Danish Animal Experimentation Board. The study complied with the Danish Animal Testing Act and the NIH Guide for the Care and Use of Laboratory Animals as well as the Animal (Scientific Procedures) Act of 1986.

Invasive arterial blood pressure

The skin over the facial and transverse facial arteries was clipped and desensitized with a topical cream containing lidocaine and prilocaine. Approximately 60 minutes later, the skin over the artery was aseptically prepared and the artery was cannulated with a 20 G, 45 mm catheter and fixed in place with glue and adhesive polster plast. Three horses could not be catheterized while standing and were anesthetized to reduce unnecessary pain and distress from the procedure. These horses were premedicated with xylazine (1.0 mg/kg IV) and atropine (0.005 mg/kg IV). Anesthesia was induced using ketamine (2.2 mg/kg IV).¹⁹ One horse was excluded from the study at this point, as arterial catheterization was not successful. Anesthetized horses were recovered from anesthesia, and rested for 5 hours before proceeding with the experimental protocol.

All catheters were flushed with heparinized isotonic saline before insertion and were connected to a pressure transducer using a 2 m noncompliant connection line. The pressure transducer was connected to a 1 L bag containing lactated Ringer’s solution and maintained at a pressure of 300 mm Hg using a pressure infusor bag. The pressure transducer was connected to a monitor with recent factory calibration. The pressure transducer was placed at the level of the point of the shoulder as an estimate for the location of the right atrium of the horse. The system was zeroed to atmospheric pressure approximately every hour. If the arterial trace was flattened and dampened, the system was flushed and the arterial trace subjectively assessed again. The distance from the transducer to the ground was measured and recorded in cm. A 16 G 6 cm catheter was placed in the left jugular vein. Direct arterial BP was calculated and displayed by the BP monitor.

Oscillometric NIBP

The circumference of the tail base was measured to ensure that the bladder of the BP cuff was approximately 40% of the width of the tail.²⁰ Distance from the tail
Tail-cuff blood pressures in horses

Table 1: Agreement analysis and descriptive statistics across all conditions and for normo hypertension and subnormal pressure

<table>
<thead>
<tr>
<th>Conditions</th>
<th>Agreement</th>
<th>Descriptive statistics</th>
</tr>
</thead>
<tbody>
<tr>
<td></td>
<td>LCL*</td>
<td>UCL**</td>
</tr>
<tr>
<td>MAP</td>
<td></td>
<td></td>
</tr>
<tr>
<td>All conditions</td>
<td>−23</td>
<td>15</td>
</tr>
<tr>
<td>Subnormal BP</td>
<td>−19</td>
<td>18</td>
</tr>
<tr>
<td>Normotension</td>
<td>−18</td>
<td>10</td>
</tr>
<tr>
<td>Hypertension</td>
<td>−29</td>
<td>11</td>
</tr>
<tr>
<td>Subnormal BP</td>
<td>−43</td>
<td>27</td>
</tr>
<tr>
<td>Normotension</td>
<td>−31</td>
<td>28</td>
</tr>
<tr>
<td>Hypertension</td>
<td>−28</td>
<td>17</td>
</tr>
<tr>
<td>SAP</td>
<td></td>
<td></td>
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<tr>
<td>All conditions</td>
<td>−34</td>
<td>21</td>
</tr>
<tr>
<td>Subnormal BP</td>
<td>−27</td>
<td>18</td>
</tr>
<tr>
<td>Normotension</td>
<td>−37</td>
<td>25</td>
</tr>
<tr>
<td>Hypertension</td>
<td>−40</td>
<td>18</td>
</tr>
<tr>
<td>DAP</td>
<td></td>
<td></td>
</tr>
<tr>
<td>All conditions</td>
<td>−35</td>
<td>22</td>
</tr>
<tr>
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<tr>
<td>Hypertension</td>
<td>−40</td>
<td>18</td>
</tr>
</tbody>
</table>

All values are in mm Hg.

*Lower limits of agreement.
**Upper limits of agreement.
***Bias (accuracy) based on the Bland–Altman analysis.
†Precision; standard deviation (SD) of the bias (precision).
¹Mean invasive arterial BP (IBP) value.
²Maximum noninvasive BP (NIBP) value. Standard deviation (SD) of the IBP.
$%\text{Percentage of error: } 2 \times \text{precision/mean.}$

MAP, mean arterial pressure; DAP, diastolic arterial pressure; SAP, systolic arterial pressure.

base to the floor was measured and recorded in centimeter. The NIBP cuff was snugly applied to the tail base with the bladder centered over the middle coccygeal artery.1,3 Systolic, diastolic, and mean arterial BPs were obtained using the oscillometric NIBP measured by the same monitor. The hydrostatic effect on the vertical distance between the cuff and right atrial level was corrected by adding 0.736 mm Hg for each centimeter of height difference to the NIBP measurements.21

Experimental design
Heart rate and rhythm was monitored with an ECG, and the heart was ausculted simultaneously after application to ensure correlation between heart rate and ECG. Oscillometric and invasive arterial BP were measured every 2 minutes for 14 consecutive measurements for each of 3 conditions reflecting normal BP, subnormal BP, and hypertension. After application of the tail cuff, 5 acclimatizing recordings were collected before initiating data collection. If the machine did not record a measurement, the data point was discarded and the following data point was used until a total of 14 data points were achieved.

The BP of all horses was initially measured during normotension. Subsequently, hypertension was induced using a 1 mg/mL dobutamine solution administered at a rate of 0.6 μg/kg/min.22 If the BP did not increase or if a persistent 2nd degree AV block was observed on the ECG, a 0.02 mg/kg IV bolus of atropine was given once. The dobutamine infusion was discontinued when the invasive SAP reached 275 mm Hg. The last 14 paired measurements before the infusion was discontinued were used for analysis. A rest period of 4 hours was allowed for wash out before induction of a lower BP with a single IV injection of acepromazine at 0.1–0.2 mg/kg.23 Measurements commenced when a decrease for IBP was observed to be below a MAP of 90 mm Hg. If the MAP did not drop below 90 mm in 30 minutes, the first value below 100 mm Hg was used, and the measurements continued thereafter for 30 minutes.

Statistical analysis
Statistical analysis was performed using the open-source software R version 2.15.0 with the pastecs package for descriptive statistics and the MethComp package for computation of method agreement. Agreement analysis corrected for replicated measurements on each horse was performed, with accuracy defined as the mean difference (bias) between the methods. Precision was defined as the SD of the accuracy. Upper and lower limits of agreement were calculated as described by Bland and Altman modified with a random effect of horse by replicate as described by Carstensen et al. The percentage of error was calculated as $2 \times \text{SD/mean.}$

Results
A total of 252 pairs of IBP and NIBP measurements were obtained from 7 horses. Five of these horses were treated with atropine during the dobutamine infusion.

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Figure 1: Bland–Altman agreement plot of mean arterial pressure (MAP) for invasive arterial BP (IBP) compared to noninvasive oscillometric blood pressure (NIBP) across normal BP, subnormal BP, and hypertension. The lines are regressed to fit the skewed distribution.

The heart rate for the horses during normotension were (mean ± SD) 34 ± 5 beats per minute (bpm), 54 ± 16 bpm during dobutamin infusion and 35 ± 6 bpm for injection with acepromazine.

Agreement and descriptive statistics for SAP, MAP, and DAP are listed in Table 1. The IBP MAP measurements ranged from 78 to 210 mm Hg, (130 ± 14 mm Hg). The MAP after acepromazine injection ranged from 78 to 110 mm Hg (94 ± 6 mm Hg), the MAP for normotension ranged from 94 to 140 mm Hg, (120 ± 11 mm Hg), and the hypertensive MAP ranged from 130 to 210 mm Hg (170 ± 18 mm Hg). Across all BP conditions, the IBP SAP ranged from 100 to 312 mm Hg and the IBP DAP ranged from 55 to 178 mm Hg. The oscillometric NIBP device did not reliably display NIBP measurements for horses during periods of 2nd degree AV block and resumed to NIBP measurements once the AV block resolved following administration of atropine. The measured tail circumferences ranged from 19 to 24 cm with a mean of 21 ± 2 cm. This resulted in a cuff width-to-tail circumference ratio ranging from 0.60 to 0.48. When using the mean tail circumference of 21 cm, the cuff width-to-tail circumference was 0.55.

The accuracy and precision across all BP values and for each of the specific BP targets are described in Table 1. The accuracy for the NIBP MAP across all BP values, using the IBP as a reference standard, was −4 mm Hg, with a precision of 10 mm Hg and percentage error of 15%. The accuracy for NIBP SAP across all BP measurements was −8 mm Hg, with a precision of 17 mm Hg and percentage error of 21%. For NIBP DAP, the accuracy across all conditions was −8 mm Hg, with a precision of 14 mm Hg and a percentage error of 28%.

A regression line fitted to the bias of MAP (Figure 1), SAP (Figure 2), and DAP (Figure 3) as a function of the average of IBP and NIPB show an increased negative bias as the BP increased, with a more negative slope for SAP compared to MAP. In addition, SAP and DAP have wider limits of agreement compared to MAP (Figures 1–3). The mean (±SD) heart rate during normotension was 34 ± 5/min during induction of subnormal BP, it was 35 ± 6/min and for hypertension it was 55 ± 17/min. Horses receiving a dose of 0.2 mg/kg acepromazine became restless and started to pace in their stalls, while the infusion of dobutamine did not influence the behavior of any horses.
**Discussion**

The accuracy of oscillometric NIBP measurement of MAP in this study (using DABP as the reference standard) was $-4$ mm Hg, while the overall precision was 10 mm Hg. Oscillometric MAP had the lowest measurement error (12%–15%) during normotension and hypertension, with a larger error during measurement of subnormal BP. The oscillometric SAP had a larger error during subnormal pressure conditions whereas DAP measurement was accurate but imprecise across all BP ranges. These data suggest that oscillometric NIBP is an acceptable method for monitoring MAP in the standing, conscious horse.

Nout et al\textsuperscript{13} conducted a method agreement study of IBP versus oscillometric NIBP in 10 anesthetized and 4 conscious foals, and reported that the bias for MAP was $-0.5$ mm Hg, compared to $-4$ mm Hg in the present study. The report also demonstrated a lower limit of agreement for MAP of $-17$ mm Hg and the upper limit of agreement to be 16 mm Hg, compared to slightly wider limits of agreement in the current study, of $-23$ mm Hg to 15 mm Hg. Nout et al\textsuperscript{13} had lower accuracy and precision for NIBP measurement of SAP and DAP, but the limits of agreement were slightly narrower for systolic pressure ($-18$ to 48 mm Hg) compared to the present report ($-43$ to 27 mm Hg). The limits of agreement for DAP were also narrower ($-18$ to 17 mm Hg) compared to this study ($-34$ to 21 mm Hg).

Lower heart rates, particularly if accompanied by arrhythmias such as sinus bradycardia or AV block can result in inaccuracies in oscillometric NIBP measurement.\textsuperscript{30} Adult horses have a lower heart rate than foals and, as demonstrated in this study, can frequently suffer from AV block, which could explain why Nout et al\textsuperscript{13} had a lower bias for MAP compared to this report. In addition, including linked replicates on each horse widens the limits of agreement.\textsuperscript{27} There was a markedly higher percentage of error for oscillometric MAP and SAP measurement during

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**Figure 2**: Bland–Altman agreement plot of systolic arterial pressure (SAP) for Invasive arterial BP (IBP) compared to noninvasive oscillometric blood pressure (NIBP) across normal BP, subnormal BP, and hypertension. The lines are regressed to fit the skewed distribution. One outlier is outside the plot area.
Figure 3: Bland–Altman agreement plot of diastolic arterial pressure (DAP) for invasive arterial BP (IBP) compared to noninvasive oscillometric blood pressure (NIBP) across normal BP, subnormal BP, and hypertension. The lines are regressed to fit the skewed distribution. One outlier is outside the plot area.

subnormal BP, which raises concern for the accuracy of NIBP measures in clinical patients with low BP, and this phenomenon may be even more pronounced with MAP <60 mm Hg. The explanation for this is probably related to the technical function of the tested oscillometric device.

The induction of hypotension by administration of acepromazine proved to be difficult in this study. Monitoring was carried out for an hour to ensure the full efficacy of the drug,23,31 but the lowest recorded MAP was 78 mm Hg, which does not meet traditional definitions for hypotension (usually 60 mm Hg or less).5 This could be explained by the fact that the horses were euvoemic and possessed an intact sympathetic nervous system that allowed the body to compensate for mild to moderate reductions in SVR or because there was a prolonged effect of the dobutamine. Despite hypotension not being achieved in this study, the ranges of MAP studied in the subnormal, normo- and hypertensive groups are different, and a minor change in pressure range was achieved. Leise et al32 achieved comparable pressures using an acepromazine dose of 0.04 mg/kg IM, while Parry et al31 reported MAP as low as 67 mm Hg in horses using acepromazine at a dose of 0.1 mg/kg IV.

European recommendations for human NIBP devices define an accuracy ≤5 mm Hg as very accurate, 6–10 mm Hg as slightly inaccurate, 11–15 mm Hg as moderately inaccurate, and variability of >15 mm Hg is very inaccurate.33 Using this definition, the oscillometric NIBP MAP from the device studied in this report can be considered very accurate during subnormal BP and normotension, but slightly inaccurate in horses with hypertension.

The specific algorithms and cuff designs that are used in different oscillometric NIBP machines may contribute to variability, when compared to IBP measurements. A recent comparison of three NIBP devices in
hypertensive dogs demonstrated wide limits of agreement that led to categorization of individual dogs into different BP groups depending on the apparatus used. When comparing IBP to NIBP, it is also important to remember that the device’s outcome measurements are not directly comparable because IBP directly measures SAP and DAP and calculates MAP whereas oscillometric NIBP devices measure MAP and calculate SAP and DAP. Oscillometric NIBP also calculates an average MAP over several heart beats, whereas IBP measurements reflect the beat-to-beat variation and momentary changes in head height, thereby increasing the variability between the methods.

There are a number of other limitations of the current study. Compared with a previous study in horses, the cuff size used in the present experimental design resulted in a larger cuff width-to-tail circumference ratio (mean of 0.57 ± 0.05). Latshaw et al. reported that the optimal ratio was approximately 0.2, while other veterinary studies have reported 0.5 and 0.3 in dogs and 0.3 in cats.

Another important limitation of the current study is that all horses used were clinically healthy. Cardiovascular regulatory factors may vary in the critically ill or painful horse, which may alter the performance of oscillometric monitors in these cases. Future studies comparing the same oscillometric device to IBP in clinically ill horses are warranted to verify appropriate NIBP function in these situations. These studies are important because hypotension in the clinical setting is often caused by hypovolemia, and not by vasodilation as in the present study. A better model of hypotension could be achieved with experimental hypovolemia; however, based on the results in our study, we suspect that the oscillometric NIBP monitor would have low accuracy in this model. Assessment of hypotension in critically ill cases using the tested NIBP monitor should be performed cautiously, as the monitor became less accurate and precise with subnormal BP.

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Footnotes

References

Tail-cuff blood pressures in horses

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